

Corrosion behavior of self-ligating and conventional metal brackets

Lúcio Henrique Esmeraldo Gurgel Maia¹, Hibernon Lopes Filho¹, Antônio Carlos de Oliveira Ruellas²,
Mônica Tirre de Souza Araújo², Delmo Santiago Vaitsman³

Objective: To test the null hypothesis that the aging process in self-ligating brackets is not higher than in conventional brackets.

Methods: Twenty-five conventional (GN-3M/Unitek; GE-GAC; VE-Aditek) and 25 self-ligating (SCs-3M/Unitek; INs-GAC; ECs-Aditek) metal brackets from three manufacturers (n = 150) were submitted to aging process in 0.9% NaCl solution at a constant temperature of $37 \pm 1^\circ\text{C}$ for 21 days. The content of nickel, chromium and iron ions in the solution collected at intervals of 7, 14 and 21 days was quantified by atomic absorption spectrophotometry. After the aging process, the brackets were analyzed by scanning electron microscopy (SEM) under 22X and 1,000X magnifications.

Results: Comparison of metal release in self-ligating and conventional brackets from the same manufacturer proved that the SCs group released more nickel ($p < 0.05$) than the GN group after 7 and 14 days, but less chromium ($p < 0.05$) after 14 days and less iron ($p < 0.05$) at the three experimental time intervals. The INs group released less iron ($p < 0.05$) than the GE group after 7 days and less nickel, chromium and iron ($p < 0.05$) after 14 and 21 days. The ECs group released more nickel, chromium and iron ($p < 0.05$) than the VE group after 14 days, but released less nickel and chromium ($p < 0.05$) after 7 days and less chromium and iron ($p < 0.05$) after 21 days. The SEM analysis revealed alterations on surface topography of conventional and self-ligating brackets.

Conclusions: The aging process in self-ligating brackets was not greater than in conventional brackets from the same manufacturer. The null hypothesis was accepted.

Keywords: Corrosion. Orthodontic brackets. Metal.

¹PhD resident of Orthodontics, Federal University of Rio de Janeiro (UFRJ).

²Associate professor, Department of Pediatric Dentistry and Orthodontics, UFRJ.

³Adjunct professor, Department of Analytical Chemistry, LaDA - IQ/UFRJ.

» The authors report no commercial, proprietary or financial interest in the products or companies described in this article.

How to cite this article: Maia LHEG, Lopes Filho H, Ruellas ACO, Araújo MTS, Vaitsman DS. Corrosion behavior of self-ligating and conventional metal brackets. *Dental Press J Orthod.* 2014 Mar-Apr;19(2):108-14. doi: <http://dx.doi.org/10.1590/2176-9451.19.2.108-114.oar>

Submitted: September 19, 2012 - **Revised and accepted:** December 05, 2012

Contact address: Mônica Tirre de Souza Araújo
Avenida Professor Rodolpho Paulo Rocco, 325 – Ilha do Fundão – Departamento de Ortodontia / UFRJ. CEP: 21941-590 – Rio de Janeiro/RJ – Brazil
E-mail: monicatirre@uol.com.br

INTRODUCTION

Metal alloys are frequently used in Orthodontics to fabricate brackets, bands, wires and tubes. These alloys are made of austenitic stainless steel,^{1,2} such as AISI 303, 304 and 316L,³ and have nickel, chromium and iron in their composition.

When exposed to the oral environment, metal orthodontic accessories are subjected to degradation, such as corrosion by pits, fracture due to fatigue, increase in the coefficient of friction or microbiological degradation.^{4,5} When the corrosive process occurs, metal ions are released into the oral medium or transformed into oxides.²

Self-ligating brackets have been widely used during the last decade by supposing that they have advantages⁶ such as reduced treatment time as a result of reduced friction, and a more irregular morphology due to the connection system and larger volume in comparison with conventional brackets. For this reason, it is possible that they are more susceptible to corrosion.

Orthodontic appliance biodegradation is undesirable, and can hinder sliding mechanics,⁷ cause reactions of hypersensitivity due to the release of nickel and chromium,^{8,9} stain the enamel as a result of incorporating metal ions,¹⁰ or even damage the appliance.² In self-ligating brackets, corrosion is also capable of altering the connection system and reducing its effectiveness.¹¹ In the active ligation system, it may hinder the capacity of pressing the wire into the slot.¹¹ Conversely, in the passive one, it may hamper opening or closing of the connection system.¹²

The aim of this study was to assess the aging process in conventional and self-ligating metal brackets. To this end, the null hypothesis assumed that the aging process in self-ligating brackets is not greater than in conventional brackets.

MATERIAL AND METHODS

Table 1 shows the distribution of the analyzed samples. The sample consisted of 150 metal brackets, 75 self-ligating and 75 conventional for maxillary right central incisors, from three different manufacturers (3M Unitek, Aditek and GAC) (25 brackets each). The conventional brackets were Gemini (3M/Unitek, Monrovia, CA, USA), Generus (GAC, Islandia, NY, USA) and Vector (Aditek, Cravinhos, SP, Brazil); whereas the self-ligating brackets were Smart Clip (3M/Unitek), In Ovation R (GAC) and Easy Clip (Aditek).

The 25 brackets of each group were divided into five subgroups, with an equal number of samples each, numbered from one to five.

The brackets of each subgroup were stored in previously sterilized Petri dishes, without coming into contact with one another. They were subjected to corrosion in 20 ml of sterile 0.9% NaCl solution^{13,14} for a period of 21 days. The Petri dishes were kept in an incubator (Quimis - Quimis Aparelhos Científicos LTDA., Diadema-SP, Brazil) at an unchanged temperature of $37 \pm 1^\circ\text{C}$.¹⁵ Every 7 days \pm 1 hour, the brackets were removed and transferred to another container filled with a new solution.^{1,13}

At the end of each experimental time interval (7 days, 14 days and 21 days), the solution remaining in each container was analyzed by atomic absorption spectrophotometry in a Varian spectrophotometer, Model AA-1475 (Varian Indústria e Comércio Ltda., São Paulo/SP, Brazil) with a view to determining their nickel, chromium and iron contents.

At the end of the experiment, five brackets from each group (one from each subgroup) were randomly selected and their surface topography was analyzed by scanning electron microscopy – SEM (Jeol JSM 6460 LV, Japan) and compared with the surface of new brackets.

Table 1 - Distribution of samples.

Bracket	n	Group	Ligation system	Manufacturer	Reference	Lot
Gemini	25	GN	Conventional	3M / Unitek	119-713	019329500
Generus	25	GE		GAC	31-212-32	B479
Vector	25	VE		Aditek	12.32.411	100329
Smart clip	25	SCs	Self ligating	3M / Unitek	004-302	016560600B
In Ovation R	25	INs		GAC	89-112-00	B3Y7
Easy clip	25	ECs		Aditek	13.32.011	090303

SEM was operated at 20 kV, and readouts were taken under 22X and 1,000X magnification. The 22X magnification allowed a complete view of the bracket. The 1,000X magnification was performed at the slot of each bracket with the connection system opened so as to analyze the area for wire insertion. No treatment was performed on the brackets at the end of the experiment in order to prevent any possible oxides, deposited on

the bracket surface as a result of the corrosion process, from being removed. Energy-dispersive X-ray spectroscopy (EDS) was used to identify atypical depositions on bracket surface.

In each group and at each time interval, nickel, chromium and iron concentrations as well as the total amount released during the experiment were statistically assessed. The Kolmogorov-Smirnov test was used to verify the

Table 2 - Nickel content (PPM) after the different experimental time intervals.

Group	Nickel release (PPM)											
	7 days			14 days			21 days			Total		
Mean \pm SD	Intra. Sig.	Inter. Sig.	Mean \pm SD	Intra. Sig.	Inter. Sig.	Mean \pm SD	Intra. Sig.	Inter. Sig.	Mean \pm SD	Intra. Sig.	Inter. Sig.	
GN	0.00	a	A	0.00	a	A	0.00	a	A	0.0 (0.0)	A	
GE	0.14 \pm 0.28	a	ABC	0.92 \pm 0.03	b	B	0.68 \pm 0.02	b	B	1.74 \pm 0.27	B	
VE	0.53 \pm 0.03	a	B	0.00 \pm 0.01	b	A	0.00 \pm 0.01	b	A	0.54 \pm 0.03	C	
SCs	0.11 \pm 0.03	a	C	0.07 \pm 0.01	b	C	0.00	c	A	0.18 \pm 0.01	D	
INs	0.14 \pm 0.01	a	C	0.39 \pm 0.02	b	D	0.00 \pm 0.01	c	A	0.54 \pm 0.03	C	
ECs	2.79 \pm 0.03	a	D	1.24 \pm 0.03	b	E	0.00 \pm 0.01	c	A	4.03 \pm 0.03	E	

Identical letters reveal no statistical difference ($p > 0.05$). Intragroup significance - Comparison of the different time intervals in each group with ANOVA test and Tukey post hoc-test. Intergroup Significance - Comparison among the groups in each time interval with Kruskal-Wallis test and Wilcoxon post hoc-test.

Table 3 - Chromium content (PPM) after the different experimental time intervals.

Group	Chromium release (PPM)											
	7 days			14 days			21 days			Total		
Mean \pm SD	Intra. Sig.	Inter. Sig.	Mean \pm SD	Intra. Sig.	Inter. Sig.	Mean \pm SD	Intra. Sig.	Inter. Sig.	Mean \pm SD	Intra. Sig.	Inter. Sig.	
GN	0.50 \pm 0.11	a	AB	1.03 \pm 0.01	b	A	1.68 \pm 0.03	c	A	3.21 \pm 0.12	AB	
GE	0.89 \pm 0.10	a	C	1.29 \pm 0.02	b	B	1.95 \pm 0.03	c	B	4.13 \pm 0.10	C	
VE	1.15 \pm 0.02	a	D	1.03 \pm 0.05	b	A	1.95 \pm 0.06	c	B	4.13 \pm 0.11	C	
SCs	0.45 \pm 0.01	a	A	0.30 \pm 0.03	a	C	2.05 \pm 0.35	b	AB	2.81 \pm 0.33	D	
INs	0.76 \pm 0.02	a	C	1.03 \pm 0.08	b	A	1.42 \pm 0.02	c	C	3.21 \pm 0.09	A	
ECs	0.63 \pm 0.02	a	B	1.55 \pm 0.03	b	D	1.16 \pm 0.03	c	D	3.34 \pm 0.05	B	

Identical letters indicate no statistical difference ($p > 0.05$). Intragroup significance - Comparison of the different time intervals in each group with ANOVA test and Tukey post hoc-test. Intergroup Significance - Comparison among the groups in each time interval with Kruskal-Wallis test and Wilcoxon post hoc-test.

Table 4 - Iron content (PPM) after the different experimental time intervals.

Group	Iron release (PPM)											
	7 days			14 days			21 days			Total		
Mean \pm SD	Intra. Sig.	Inter. Sig.	Mean \pm SD	Intra. Sig.	Inter. Sig.	Mean \pm SD	Intra. Sig.	Inter. Sig.	Mean \pm SD	Intra. Sig.	Inter. Sig.	
GN	0.35 \pm 0.03	a	A	0.44 \pm 0.03	b	A	1.02 \pm 0.02	c	A	1.81 \pm 0.04	A	
GE	0.93 \pm 0.05	a	B	1.02 \pm 0.02	b	B	1.28 \pm 0.02	c	B	3.23 \pm 0.08	B	
VE	1.01 \pm 0.05	a	B	0.77 \pm 0.04	b	C	1.02 \pm 0.02	a	A	2.80 \pm 0.09	CD	
SCs	0.00 \pm 0.01	a	C	0.01 \pm 0.02	a	D	0.94 \pm 0.02	b	C	0.96 \pm 0.04	E	
INs	0.77 \pm 0.02	a	D	0.94 \pm 0.02	b	E	1.01 \pm 0.03	c	A	2.72 \pm 0.02	C	
ECs	1.02 \pm 0.03	a	B	0.94 \pm 0.02	b	E	0.94 \pm 0.04	b	D	2.90 \pm 0.08	D	

Identical letters indicate no statistical difference ($p > 0.05$). Intragroup significance - Comparison of the different time intervals in each group with ANOVA test and Tukey post hoc-test. Intergroup Significance - Comparison among the groups in each time interval with Kruskal-Wallis test and Wilcoxon post hoc-test.

sample normality of distribution. As normal distribution was not found, the non-parametric ANOVA test with Tukey post-test were applied for intragroup assessment, whereas the Kruskal-Wallis test with Wilcoxon post-test were applied for intergroup assessment. The data were statistically analyzed using SPSS 17.0 software (Statistical Package for Social Sciences, SPSS Inc., Chicago, IL, USA). The significance level was set at 5%.

RESULTS

During the experimental period, the release of nickel, chromium and iron metal ions was observed in all groups, except for nickel ion in the GN group, which was not detected at any of the time intervals (Tables 2, 3 and 4).

There was greater release of nickel in the initial period of the experiment, both for conventional and self-ligating brackets, with a trend towards no release of this ion at the end of the experiment ($p < 0.05$). Only group GN and group GE behaved differently with greater release of nickel on the 14th and 21st days. The

experimental groups revealed a trend towards increasing release of ions, such as chromium and iron, from the first to the third week of the experiment ($p < 0.05$). The only exception was group VE, in which a great amount of iron release was found in the first week. Metal release was similar in self-ligating and conventional brackets from the same manufacturer. Group SCs released more nickel ($p < 0.05$) than group GN after 7 and 14 days, but group GN released more chromium ($p < 0.05$) after 14 days and more iron ($p < 0.05$) at the three experimental time intervals. Group INs released less iron ($p < 0.05$) than group GE after 7 days; and less nickel, chromium and iron ($p < 0.05$) after 14 and 21 days. Group ECs released more nickel, chromium and iron ($p < 0.05$) than group VE after 14 days, but released less nickel and chromium ($p < 0.05$) after 7 days and less chromium and iron ($p < 0.05$) after 21 days.

At the end of the experiment, the SEM analysis revealed that the surface topography of all brackets changed, with signs of aging when compared with the surface of new brackets (Figs 1 to 4).

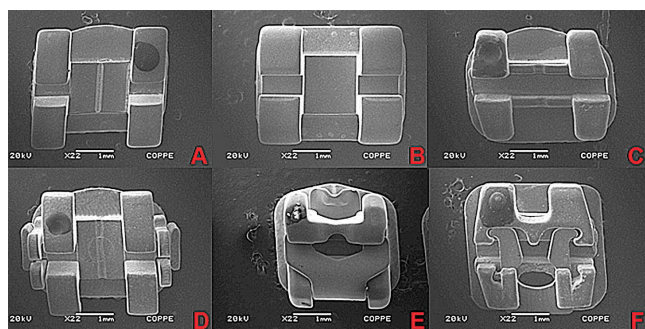


Figure 1 - Surface topography of new brackets visualized by SEM under 22X magnification. A) GN; B) GE; C) VE; D) SCs; E) INs; F) ECs.

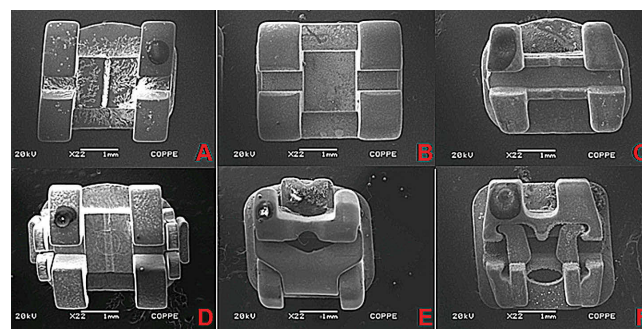


Figure 2 - Surface topography of brackets visualized by SEM under 22X magnification after 21 days. A) GN; B) GE; C) VE; D) SCs; E) INs; F) ECs.

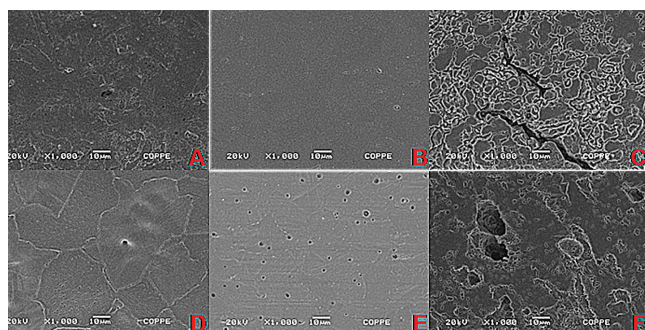


Figure 3 - Surface topography of new brackets visualized by SEM under 1000X magnification. A) GN; B) GE; C) VE; D) SCs; E) INs; F) ECs.

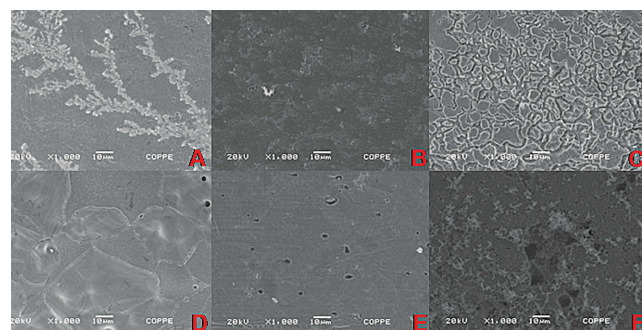


Figure 4 - Surface topography of brackets visualized by SEM under 1000X magnification after 21 days. A) GN; B) GE; C) VE; D) SCs; E) INs; F) ECs.

DISCUSSION

Bracket corrosion with consequent release of metal ions during orthodontic treatment may hinder orthodontic mechanics,² trigger hypersensitivity reactions with hyperplasia and gingival tissue inflammation,^{4,8,9} and contribute to iatrogenic staining of the enamel with the incorporation of metals.^{10,16}

A corroded bracket often presents a more irregular surface and can accumulate products resulting from corrosion (Fig 4). Thus, friction between the bracket and wire during sliding mechanics increases, making it necessary to apply force of greater magnitude to overcome the friction and produce physiologic tooth movement.^{7,17,18} When excessive force is applied to the bracket, there is loss of mechanical control and increased probability of root resorption.^{5,9,19,21}

One of the advantages attributed to self-ligating brackets is the lower degree of friction that the ligation system imposes on the orthodontic wire when compared with conventional tying.^{6,22,24} However, if the bracket has an increased corrosion potential, friction also increases,²⁵ affecting this advantage.

In the present study, SEM analysis under 22X magnification (Fig 2) revealed that, in general, self-ligating brackets showed more areas with altered surface topography due to corrosion, when compared with conventional brackets from the same manufacturer, possibly due to their geometry with larger retentive areas. Thus, brackets in the INs group had a more irregular surface than the brackets in the GE group, while the brackets in the ECs group presented greater alterations in comparison to those in the VE group. The self-ligating brackets of the SCs group and the conventional brackets in group GN did not present significant alterations in their surface topography. Energy-dispersive X-ray spectroscopy (EDS) revealed NaCl deposition on the surfaces of the brackets in group GN.

Analysis of the images obtained by SEM under 1000X magnification (Figs 3 and 4) suggests that new brackets with more irregular surfaces were more susceptible to corrosion. Thus, the brackets in group ECs, which presented a surface topography with deficient smoothness and porosity at the beginning of the experiment, presented a considerably more irregular surface at the end of it. The brackets in group VE also presented considerably altered surfaces at the end of the experiment, due to the formation of oxides. Moreover, the

brackets in group INs, which presented irregularities at the beginning of the experiment, were significantly subjected to pitting corrosion. Quantification of the metal ions released during the experiment corroborates these data. These groups had great release of nickel, chromium and iron ions.

The release of metal ions into the oral environment may trigger hypersensitivity reactions.^{4,5,8,9,26} Nickel and chromium are present in the composition of brackets with the goal of increasing resistance to corrosion.^{2,4,16,27} These elements are largely responsible for the aforementioned adverse reactions. Nickel is strongly responsible for triggering more allergic reactions than any other metal.^{8,26}

Under the conditions of this experiment, the release of nickel was considerably lower than the daily ingestion of this metal through food (300 to 600 µg/day).¹³ However, it is worth noting that susceptible patients in contact with small concentrations of this metal are more likely to suffer hypersensitivity reactions.²⁹

The oral reaction of allergy to nickel is difficult to diagnose, since its clinical signs and symptoms are similar to those of gingivitis caused by poor oral hygiene. The low number of reports of hypersensitivity to nickel is possibly due to this difficulty in diagnosis. Epidemiological data point towards an incidence of sensitivity to this metal of approximately 20% in the general population.^{28,30}

Similarly to other *in vitro* studies,^{1,15,31} the release of nickel in this experiment was higher in the first two weeks, with a trend towards no further release during the third week. The exception was group GE which continued to release nickel ions during the last week (Table 2).

Similarly to previous studies,^{1,13} chromium and iron ions had a trend towards increasing release throughout the experiment in all groups, except for group ECs (Tables 3 and 4). In this group, there was a greater release of chromium in the second week, and greater release of iron in the first week, although the concentration of these ions remained high at the end of the third week.

Within the limitations and conditions of this experiment, it is reasonable to conclude that metal release was similar in self-ligating and conventional brackets from the same manufacturer.

When self-ligating and conventional brackets from the same manufacturer were compared, group SCs proved to release more nickel ($p < 0.05$) than group GN after

7 and 14 days, whereas group GN released more chromium ($p < 0.05$) after 14 days and more iron ($p < 0.05$) at the three experimental time intervals. Group INs released less iron ($p < 0.05$) than group GE after 7 days and less nickel, chromium and iron ($p < 0.05$) after 14 and 21 days. Group ECs released more nickel, chromium and iron ($p < 0.05$) than group VE after 14 days, but released less nickel and chromium ($p < 0.05$) after 7 days and less chromium and iron ($p < 0.05$) after 21 days.

Metal ions released by metal brackets and bands during orthodontic treatment may be incorporated into tooth enamel, causing iatrogenic color alteration and stains.^{10,16} In cases of severe pigmentation, restorative treatment of the vestibular surface of the stained tooth proves necessary.^{32,33} Special care must be given to patients with poor oral hygiene, since altered oral environment, with

reduced pH and presence of acidogenic microorganisms potentiates the corrosion of metal accessories. Additionally, enamel demineralization and remineralization processes may influence the incorporation of metals.^{4,10}

CONCLUSIONS

- » The null hypothesis was accepted.
- » The SEM analysis revealed that self-ligating and conventional brackets presented signs of aging.
- » Metal ions release in self-ligating brackets was similar to conventional brackets from the same manufacturer.

Acknowledgements

We deeply thank Dr. Cláudia Trindade Mattos for helping us with statistical analysis of data.

REFERENCES

1. Barrett RD, Bishara SE, Quinn JK. Biodegradation of orthodontic appliances. Part I. Biodegradation of nickel and chromium in vitro. *Am J Orthod Dentofacial Orthop.* 1993;103(1):8-14.
2. Toms AP. The corrosion of orthodontic wire. *Eur J Orthod.* 1988;10:87-97.
3. Zinelis S, Annousaki O, Eliades T, Makou M. Elemental composition of brazing alloys in metallic orthodontic brackets. *Angle Orthod.* 2004;74(3):394-9.
4. Eliades T, Athanasiou AE. In vivo aging of orthodontic alloys: implications for corrosion potential, nickel release, and biocompatibility. *Angle Orthod.* 2002;72(3):222-37.
5. House K, Sernetz F, Dymock D, Sandy JR, Ireland AJ. Corrosion of orthodontic appliances--should we care? *Am J Orthod Dentofacial Orthop.* 2008;133(4):584-92.
6. Pizzoni L, Ravnholt G, Melsen B. Frictional forces related to self-ligating brackets. *Eur J Orthod.* 1998;20(3):283-91.
7. Andreassen GF, Quevedo FR. Evaluation of friction forces in the 0.022 x 0.028 edgewise bracket in vitro. *J Biomech.* 1970;3(2):151-60.
8. Menezes LM, Campos LC, Quintão CC, Bolognese AM. Hypersensitivity to metals in orthodontics. *Am J Orthod Dentofacial Orthop.* 2004;126(1):58-64.
9. Hwang CJ, Shin JS, Cha JY. Metal release from simulated fixed orthodontic appliances. *Am J Orthod Dentofacial Orthop.* 2001;120(4):383-91.
10. Maia LHEG, Lima Filho HL, Araujo MVA, Ruellas ACO, Araujo MTS. Incorporation of metal and color alteration of enamel in the presence of orthodontic appliances. *Angle Orthod.* 2012;82(5):889-93.
11. Pandis N, Bourauel C, Eliades T. Changes in the stiffness of the ligating mechanism in retrieved active self-ligating brackets. *Am J Orthod Dentofacial Orthop.* 2007;132(6):834-7.
12. Eliades T. Self-ligating brackets malfunction: is it due to corrosion? *Orthod Mat Insider.* 2009;21:4-7.
13. Grimsdottir MR, Gjerdet NR, Hensten-Pettersen A. Composition and in vitro corrosion of orthodontic appliances. *Am J Orthod Dentofacial Orthop.* 1992;101(6):525-32.
14. Kerosuo H, Moe G, Kleven E. In vitro release of nickel and chromium from different types of simulated orthodontic appliances. *Angle Orthod.* 1995;65(2):111-6.
15. Park HY, Shearer TR. In vitro release of nickel and chromium from simulated orthodontic appliances. *Am J Orthod.* 1983;84(2):156-9.
16. Majier R, Smith DC. Corrosion of orthodontic bracket bases. *Am J Orthod.* 1982;81(1):43-8.
17. Angolkar PV, Kapila S, Duncanson MG Jr, Nanda RS. Evaluation of friction between ceramic brackets and orthodontic wires of four alloys. *Am J Orthod Dentofacial Orthop.* 1990;98(6):499-506.
18. Kapila S, Angolkar PV, Duncanson MG Jr, Nanda RS. Evaluation of friction between edgewise stainless steel brackets and orthodontic wires of four alloys. *Am J Orthod Dentofacial Orthop.* 1990;98(2):117-26.
19. Drescher D, Bourauel C, Schumacher HA. Frictional forces between bracket and arch wire. *Am J Orthod Dentofacial Orthop.* 1989;96(5):397-404.
20. Lin MC, Lin SC, Lee TH, Huang HH. Surface analysis and corrosion resistance of different stainless steel orthodontic brackets in artificial saliva. *Angle Orthod.* 2006;76(2):322-9.
21. Reitan K. Initial tissue behavior during apical root resorption. *Angle Orthod.* 1974;44(1):68-82.
22. Berger JL. The influence of the SPEED bracket's self-ligating design on force levels in tooth movement: a comparative in vitro study. *Am J Orthod Dentofacial Orthop.* 1990;97(3):219-28.
23. Thorstenson GA, Kusy RP. Resistance to sliding of self-ligating brackets versus conventional stainless steel twin brackets with second-order angulation in the dry and wet (saliva) states. *Am J Orthod Dentofacial Orthop.* 2001;120(4):361-70.
24. Thomas S, Sherriff M, Birnie D. A comparative in vitro study of the frictional characteristics of two types of self-ligating brackets and two types of pre-adjusted edgewise brackets tied with elastomeric ligatures. *Eur J Orthod.* 1998;20(5):589-96.
25. Marques IS, Araujo AM, Gurgel JA, Normando D. Debris, roughness and friction of stainless steel archwires following clinical use. *Angle Orthod.* 2010;80(3):521-7.
26. Bishara SE, Barrett RD, Selim MI. Biodegradation of orthodontic appliances. Part II. Changes in the blood level of nickel. *Am J Orthod Dentofacial Orthop.* 1993;103(2):115-9.
27. Majier R, Smith DC. Biodegradation of the orthodontic bracket system. *Am J Orthod Dentofacial Orthop.* 1986;90(3):195-8.
28. Bass JK, Fine H, Cisneros GJ. Nickel hypersensitivity in the orthodontic patient. *Am J Orthod Dentofacial Orthop.* 1993;103(3):280-5.
29. Prystowsky SD, Allen AM, Smith RW, Nonomura JH, Odom RB, Akers WA. Allergic contact hypersensitivity to nickel, neomycin, ethylenediamine, and benzocaine. Relationships between age, sex, history of exposure, and reactivity to standard patch tests and use tests in a general population. *Arch Dermatol.* 1979;115(8):959-62.
30. Kerosuo H, Kullaa A, Kerosuo E, Kanerva L, Hensten-Pettersen A. Nickel allergy in adolescents in relation to orthodontic treatment and piercing of ears. *Am J Orthod Dentofacial Orthop.* 1996;109(2):148-54.
31. Menne T, Brandup F, Thestrup-Pedersen K, Veien NK, Andersen JR, Yding F, et al. Patch test reactivity to nickel alloys. *Contact Dermatitis.* 1987;16(5):255-9.
32. Romano FS, Correr Sobrinho L, Consani S, Araújo MBB, Nouer DF. Oxidação de bráquetes metálicos. *Rev Dental Press Ortod Ortop Facial.* 2005;10(6):24-5.
33. Hodges SJ, Spencer RJ, Watkins SJ. Unusual indelible enamel staining following fixed appliance treatment. *J Orthod.* 2000;27(4):303-6.